Please amend the specification at paragraph [0045] of the published application:

[0045] The bioresorbable stents then undergo an annealing process. The annealing process includes placing the bioresorbable stents on a mandrel, axially compressing the stents by 30% to 60%, heating the stents to the glass transition temperature of the biocompatible polymer for a predetermined period of time, and allowing the stents to be controllably cooled. The annealing process relieves internal stresses and instabilities of the monofilaments that result from the production of the bioresorbable stents. In a preferred embodiment of the present invention where the latticed structure is formed form poly-L-lactide monofilaments, the bioresorbable stents are heated to approximately 90°C for a length of time between about one and about eight hours, preferably four hours, in an inert atmosphere. The inert atmosphere may be comprised of a high vacuum or nitrogen gas. Those skilled in the art will appreciate that other inert atmospheres having low moisture content are also contemplated including, but not limited to, argon, or helium. The bioresorbable stents are then controllably cooled to room temperature. Each stent is then cut to desired size for its intended application. Thereafter, the stents are exposed to Co^{60} gamma irradiation (for example, approximately 35 kGy to 75 kGy total dose of gamma irradiation) to fine tune the in vivo functional lifetime of the bioresorbable stents. Exposure to gamma irradiation causes molecular degradation of the polymers that comprise the bioresorbable stents; however, the gamma irradiation does not affect the overall morphology of the polymers.